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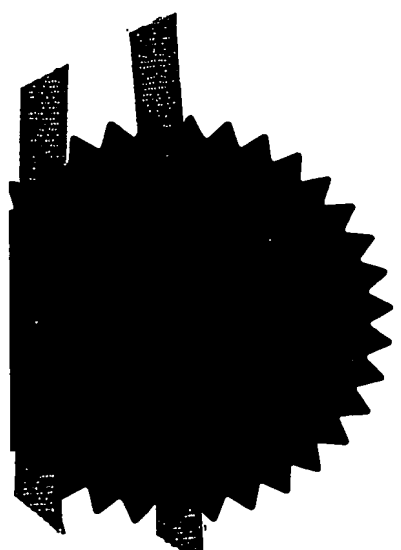
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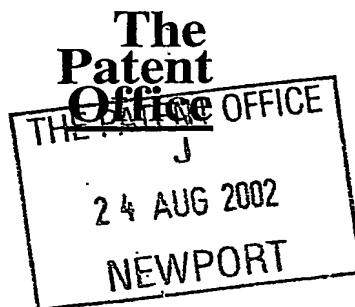
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Signed *Andrew Giersey*
Dated 18 September 2003



1/77

Request for grant of a patent

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27AUG02 E743522-1 002481
P01/7700 0.00-0219758.0

2. Patent Application Number (the Patent Office will fill in this part) 0219758.0 124 AUG 2002

3. Full name, address and postcode of the or of each applicant (underline all surnames) Grampian University Hospitals NHS Trust -and- University of Aberdeen
Foresterhill House Kings College
Ashgrove Road West Aberdeen
Aberdeen AB24 3FX
AB25 2ZB

Patents ADP number (if you know it) 783670300

If the applicant is a corporate body, give the country/state of its incorporation

United Kingdom

7131006002

4. Title of the invention "Device"

5. Name of your agent (if you have one) Murgitroyd & Company
"Address for service" in the United Kingdom to which all correspondence should be sent (including the postcode) 165 - 169 Scotland Street
Glasgow
G5 8PL

Patents ADP number (if you know it) 1198015

6. If you are declaring priority from one or more earlier patent applications, give the country and the date of filing of the or of each of these earlier applications and (if you know it) the or each application number

Country	Priority application number (if you know it)	Date of filing (day / month / year)
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7. If this application is divided or otherwise derived from an earlier UK application, give the number and the filing date of the earlier application

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Description 13

Claim(s) -

Abstract -

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Request for preliminary examination and search (Patents Form 9/77) -

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MURGITROYD & COMPANY

Date 23/08/02

12. Name and daytime telephone number of person to contact in the United Kingdom

Jamie Allan 01224 706616

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1 "Device"

2

3 This invention relates to an implantable replacement
4 joint, and typically, but not exclusively to a body-
5 implantable replacement joint to replace worn or
6 damaged joints in a body.

7

8 Joint replacement is a well established practice for
9 treating patients suffering from diseases such as
10 inflammatory arthritis or osteoarthritis. These
11 conditions can result in considerable pain, loss of
12 function, deformity and loss of quality of life.

13 The most common types of artificial implant joints
14 are used to replace worn or damaged hip joints, and
15 typically consist of a ball and socket arrangement
16 attached to bones at respective sides of the joint,
17 or flexible silicon-based bridges such as the
18 Swanson device, which is used for smaller joints
19 such as the wrist or fingers. Loosening,
20 dislocation tearing and fracture have been all
21 reported for existing implants.

22

1 According to the present invention there is provided
2 an implantable replacement joint comprising a first
3 component for attachment to a first bone portion,
4 and second component for attachment to a second bone
5 portion, and a flexible component extending between
6 the first and second components.

7
8 The first bone portion is typically located on one
9 side of a joint, and the second bone portion is
10 typically located on the other side of the joint.

11
12 The first and second components are typically
13 adapted to be anchored within cavities in the
14 respective first and second bone portions on
15 opposing sides of the joint to be replaced. The
16 first and second components can typically be
17 anchored in place using friction, and in such
18 embodiments can be shaped to be an interference fit
19 within a cavity of the first and second bone
20 portions. The cavity can be naturally occurring,
21 e.g. the intramedullary canal, or can be created
22 within a bone or group of bones to receive the first
23 and second components, as required. In alternative
24 embodiments, the first and second components can be
25 anchored into the respective bone portions using
26 adhesives, cement, grout, screw threads, or fixing
27 devices such as screws, nails or expansion devices
28 etc.

29
30 In certain embodiments the first and second
31 components have formations on their outer surfaces
32 in order to key into the inner surfaces of the

1 cavities in the first and second bone portions. The
2 formations on the outer surfaces of the first and
3 second portions can typically be screw threads,
4 annular or semi-annular ridges or simple protrusions
5 or expansion fins on the outer surfaces.

6
7 Typically the flexible component is elongate. In
8 preferred embodiments, each of the first and second
9 components has an elongate stem with a central bore
10 extending along the stem to receive a part, e.g. one
11 end, of the flexible component. In such
12 embodiments, the flexible component can thus be
13 substantially contained within a cavity formed by
14 the central bores of the first and second
15 components. Typically the cavity is longer than the
16 flexible component, so that the flexible component
17 can move axially within the cavity. Typically the
18 bores of the first and second components are wider
19 than the flexible component so that the flexible
20 component is a loose fit within the cavity. The
21 relative dimensions of the flexible component and
22 the first and second components are preferably such
23 that even if the first and second components are
24 pushed together to close any gap between the central
25 bores, the flexible component will not be compressed
26 within the cavity by the first and second
27 components.

28

29 In especially preferred embodiments, the first and
30 second components have bearing surfaces that
31 articulate against one another when the device is
32 made up. Typically the central bores and the

1 flexible component extend through the bearing
2 surfaces. The bearing surfaces can be arcuate and
3 can be adapted to promote pivotal movements of the
4 first and second components relative to one another.
5 Preferably bearing surfaces promote particular
6 pivotal movements e.g. in a particular plane.
7 Typically the arcuate portions of the respective
8 bearing surfaces on the first and second components
9 are arranged on opposite axes, so that, for example,
10 the bearing surface on the first component can be
11 convex along an x-axis, and the bearing surface on
12 the second component can be convex along a y-axis
13 intersecting the x-axis. This arrangement can be
14 extremely useful in promoting pivotal movements in
15 more than one plane, allowing the replacement joint
16 a number of degrees of freedom of movement, while
17 controlling the location of the pivot axis on the
18 device. However, it is envisaged that simple
19 embodiments of the invention can be created with
20 only one degree of freedom of movement, and without
21 curved bearing surfaces.

22
23 Typically the first and second components are made
24 from a relatively hard plastics material or carbon
25 fibre composites, and preferably from one that is
26 not biodegradable. Suitable materials for the first
27 and second components include stainless steel,
28 alloys such as cobalt chrome or titanium alloy,
29 polyethylene or other plastics materials, or
30 ceramics or carbon fibre composites. It can be
31 advantageous to use materials for the first and
32 second components that have a similar modulus to

1 bone itself, and plastics materials are particularly
2 useful in this respect.

3

4 The flexible component can be made from a resilient
5 material such as rubber, and in preferred
6 embodiments of the invention, the flexible component
7 does have some resilience. The flexible component
8 is typically formed from a relatively softer
9 material than the first and second components. The
10 flexible component can be made from e.g. silicone or
11 polyurethane and can preferably have a flexibility
12 that is intrinsic to the material used, although
13 other forms of flexible component can be used where
14 the flexibility is derived from e.g. a hinge
15 inserted into a rigid material. The material chosen
16 for the flexible portion is typically different from
17 the material chosen for the first and second
18 portions.

19

20 The flexible portion can typically have a convoluted
21 hinge made up from a convoluted or folded section of
22 the material.

23

24 In some embodiments of the invention, a bearing
25 plate can be provided between the bearing surfaces
26 of the first and second components. The bearing
27 plate can typically be of a different material from
28 the first and second components (for example, where
29 the first and second portions are made from plastics
30 material, the bearing plate can usefully be made
31 from a metal), in order to reduce wear caused by the
32 bearing surfaces of the first and second components

1 rubbing against one another. The bearing plate can
2 have arcuate surfaces if desired, but in simple
3 embodiments has generally flat faces. The bearing
4 plate can extend the range of movement that is
5 possible between the first and second components, by
6 introducing an additional pivot point, so that each
7 of the first and second components pivots on
8 opposite faces of the bearing plate. The bearing
9 plate can be formed with legs, extensions or
10 prominent edges that can generally attach the
11 bearing plate to one of the first and second
12 components. The bearing plate could also be formed
13 of plastics material, ceramics or other suitable
14 materials. Where the first and second components
15 are formed from ceramics materials, the bearing
16 plate can comprise a plastics material so as to
17 provide an interface of different materials at the
18 bearing surfaces.

19
20 The replacement joint of the invention is preferably
21 a wrist joint, but can also be used in any joint,
22 particularly fingers, toes, knees and elbows. Is
23 particularly useful to replace worn or damaged
24 joints where more than two degrees of freedom is
25 required, such as rotation of the first and second
26 components in addition to flexion/extension and
27 medial/lateral deviation.

28
29 In especially preferred embodiments of the
30 invention, the pivot axis around which the first and
31 second components move relative to one another is
32 typically movable relative to the device, and this

1 is typically achieved by the ability of the flexible
2 component to move within the bores of the first and
3 second components, thereby creating a "sloppy hinge"
4 between the first and second components. This
5 permits the first and second components to move
6 axially relative to one another while moving in
7 relative rotation and flexion/extension or in
8 medial/lateral directions. Indeed, the ability to
9 move axially while rotating, deviating laterally,
10 and flexing or extending enables the replacement
11 joint to move in a similar fashion to the natural
12 joint it is replacing. This reduces strain on the
13 anchoring points between the bone portions and the
14 first and second components, and reduces pull-out
15 failures or bone wear at the interfaces.

16

17 An embodiment of the present invention will now be
18 described by way of example, and with reference to
19 the accompanying drawings, in which;

20

21 Fig 1 is a side view of a body implantable
22 device;

23 Fig 2 is a front sectional view through the
24 device of Fig 1;

25 Fig 3 is a side view of a first component of
26 the fig 1 device;

27 Fig 4 is a front sectional view through the fig
28 3 component;

29 Fig 5 is a front view of a second component of
30 the Fig 1 device;

31 Fig 6 is a side sectional view through the fig
32 5 component;

1 Fig 7 is a side view of a bearing plate used in
2 the Fig 1 device;
3 Fig 8 is a plan view of the bearing plate;
4 Fig 9 is a side view of a flexible component of
5 the Fig 1 device;
6 Fig 10 is a perspective view of the Fig 1
7 device;
8 Fig 11 is a perspective view of the Fig 1
9 device in flexion/extension;
10 Fig 12 is a side view of the Fig 1 device in
11 flexion/extension;
12 Fig 13 is a perspective view of the Fig 1
13 device showing lateral deviation;
14 Fig 14 is a side view of the Fig 1 device
15 showing lateral deviation;
16 Fig 15 is a front view of the Fig 1 device
17 showing lateral deviation;
18 Fig 16 is a perspective view of the Fig 1
19 device showing relative rotation of the two
20 components; and
21 Fig 17 is a side view of the Fig 1 device
22 showing relative rotation of the two
23 components.

24
25 Referring now to the drawings, a body implantable
26 device designed for use as the replacement wrist
27 joint comprises a first component 5 and a second
28 component 10. The first component 5 is dimensioned
29 and adapted to be implanted within the distal end of
30 the intramedullary canal of the radius, and the
31 second component 10 is intended and adapted to be
32 implanted into a bore created in the proximal part

1 of the carpus and/or metacarpals. Each of the first
2 and second components 5,10 can have external
3 protrusions such as ridges or screw-threads (not
4 shown) to enhance retention of the component within
5 the bone portion into which it is implanted. In
6 this embodiment, each of the first and second
7 components 5,10 is sized and adapted to fit within
8 either the intramedullary canal of the radius or the
9 bore created in the carpus and/or metacarpals and to
10 form an interference fit within that cavity, so that
11 they can be retained therein merely by friction
12 between the outer surface of the components 5,10,
13 and the inner surface of the cavity in the bone(s).
14

15 With reference to fig 3 and fig 4, the first
16 component 5 comprises a tapered stem 6 adapted to
17 fit within the distal intramedullary canal of the
18 radius, and a head 7 located on top of the stem 6.
19 The head 7 has laterally extending arms and has a
20 distal convex bearing surface 8 that is curved from
21 the front of the first component 5 to the back. The
22 radius of curvature of the surface 8 is
23 approximately 16mm. The first component 5 has a
24 blind-ended bore 9 extending axially through the
25 stem 6, and presenting an aperture through the upper
26 surface 8 of the head 7.
27

28 The first and second components are made from ultra-
29 high molecular weight polyethylene.
30

31 With reference to Figs. 5 and 6 the second component
32 10 also has a tapered stem 11, and a head 12, again

1 with laterally extending arms, and a proximal
2 bearing surface 13. The proximal bearing surface 13
3 of the head 12 is also convex, but is curved from
4 one side of the second component 10 to the other
5 side. The radius of curvature of the bearing face
6 13 is approximately 65mm. The second component 10
7 has a blind-ended bore 14 extending axially through
8 the stem 11, and presenting an aperture through the
9 upper surface 13 of the head 12.

10

11 A flexible rod 15 of silicone as shown in fig 9 has
12 a central cylindrical portion and tapered ends that
13 are adapted to be received within the blind ended
14 bores 9, 14 of the first and second components 5,10
15 respectively. The length of the flexible rod is
16 typically slightly less than the combined lengths of
17 the blind ended bores 9, 14, so that when the device
18 is assembled with the first and second components
19 5,10 placed head-to-head, with the bores 9, 14
20 aligned and the arms on the respective heads
21 arranged parallel to one another, the flexible rod
22 15 can move axially within the cavity formed by the
23 two bores 9, 14.

24

25 With reference to Figs. 7 and 8, a bearing plate 17
26 formed of stainless steel is typically provided
27 between the bearing surfaces 8, 13 of the heads
28 7,12, and typically has an aperture 18 to allow
29 passage of the flexible rod 15 through the bearing
30 plate 17. The aperture 18 is aligned with the bores
31 9,14 when the device is assembled. In this
32 embodiment, the device is made up such that the

1 bearing surface 8 of the first component 5
2 articulates against one surface 17a of the bearing
3 plate 17, while the bearing surface 13 of the second
4 component 10 articulates against the opposite
5 surface 17b of the bearing plate 17. The bearing
6 plate 17 typically has arms extending from the
7 surface 17b plate to engage the side walls of the
8 head 12 of the second portion 10. It will be
9 appreciated that embodiments of the invention can
10 function satisfactorily without a bearing plate 17,
11 and that bearing plates can be used without side
12 walls.

13
14 Turning now to Figs. 10 to 17, the device is shown
15 at rest in fig 10, with the two components 5,10 in
16 axial alignment with one another with the bearing
17 plate 17 interposed. In this configuration, the
18 flexible rod 15 is not bent or energised in any way
19 and is held within the cavity formed by the bores 9,
20 14. Figs 11 and 12 show the device in flexion, with
21 the second component 10 pivoting with respect to the
22 first component 5 around the y-axis shown in fig 10.
23 Notice that the bearing plate 17 moves with the
24 second portion 10 relative to the first portion
25 5, and that the bearing surface 8 of the head 7 of
26 the first portion 5 articulates against the face 17a
27 of the bearing plate 17. The front to back
28 curvature of the bearing surface 8 promotes a smooth
29 articulation about the y-axis. The ends of the
30 flexible rod 15 remain within the bores 9, 14, and
31 the central portion of the rod 15 bends to
32 accommodate and control the flexion. Since the rod

1 15 can move axially within the cavity formed by the
2 bores 9, 14, the pivot axis formed in the central
3 portion of the rod 15 can move axially with respect
4 to the first and second portions 5,10 as the device
5 flexes, thereby allowing a greater range of movement
6 of the joint. Also, since the flexible rod 15 can
7 move within the cavity formed by the bores 9, 14,
8 the two portions 5,10 can extend relative to one
9 another along the x-axis, while undergoing flexion,
10 extension, medial/lateral deviation and/or rotation.

11

12 Figs 13, 14 and 15 show the joint moving in
13 medial/lateral deviation around the z-axis of fig
14 10, i.e. as if moving in radio-ulnar deviation when
15 in place in the body. Notice that during lateral
16 deviation around the z-axis, the bearing plate 17
17 remains with the first portion 5, and the bearing
18 surface 13 of the head 12 of the second portion 10
19 articulates against the surface 17b of the plate 17.
20 In pure lateral deviation, with no movement around
21 the y-axis, the pivotal movement of the plate 17
22 relative to the first portion 5 is negligible, and
23 the lateral movement of the first portion 10 is
24 constrained by the head 12 moving within the
25 confines of the arms of the bearing plate 17. In
26 certain circumstances, the plate 17 can move
27 relative to the first portion 5, for example, when
28 the flexible rod 15 moves axially to allow the
29 extension of the device.

30

31 Figs. 16 and 17 show relative rotational movement of
32 the two portions 5,10 around the x-axis. Notice

1 that the arms of the bearing plate 17 keep the plate
2 17 stationary with respect to the second portion 10,
3 and the two portions pivot around the axis of the
4 flexible rod 15 held straight within the central
5 cavity formed by the bores 9, 14.

6
7 Clearly is possible for the joint to carry out more
8 complex combination movements involving a
9 combination of rotation, medial/lateral deviation,
10 and extension/flexion, in any combination. It is
11 also possible for axial separation of the two
12 portions to occur during any such movement.

13
14 Modifications and improvements can be incorporated
15 without departing from the scope of the invention ..

16

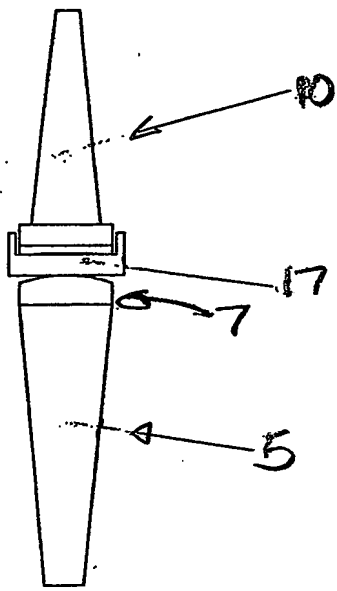


Figure 1

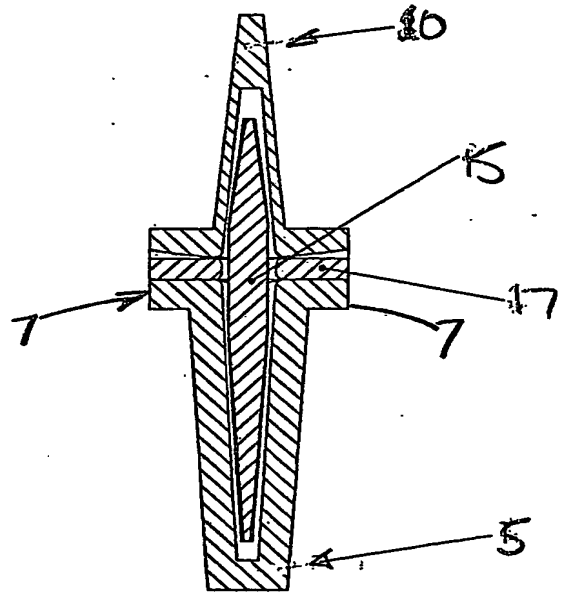


Figure 2

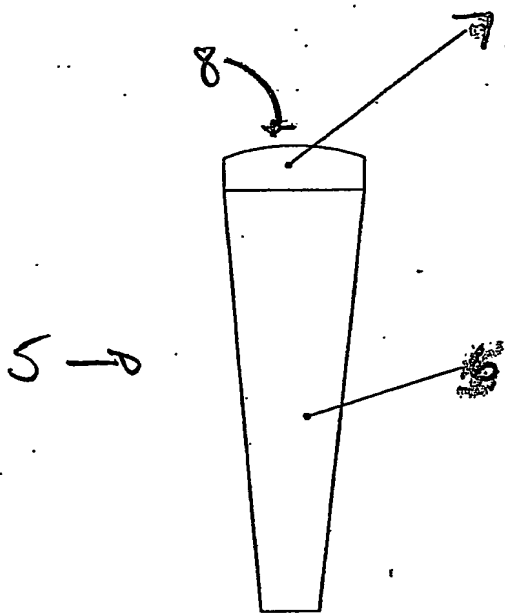


Figure 3

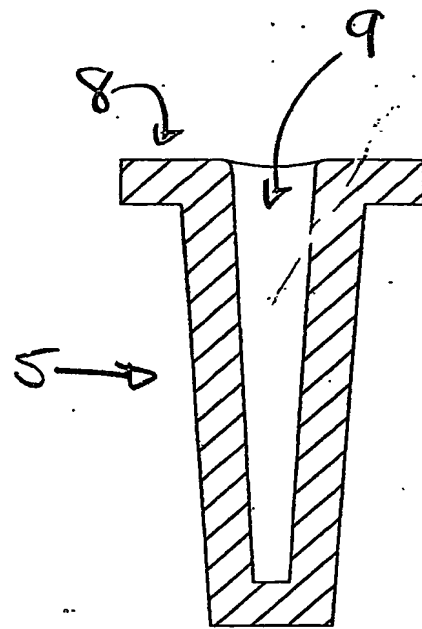


Figure 4

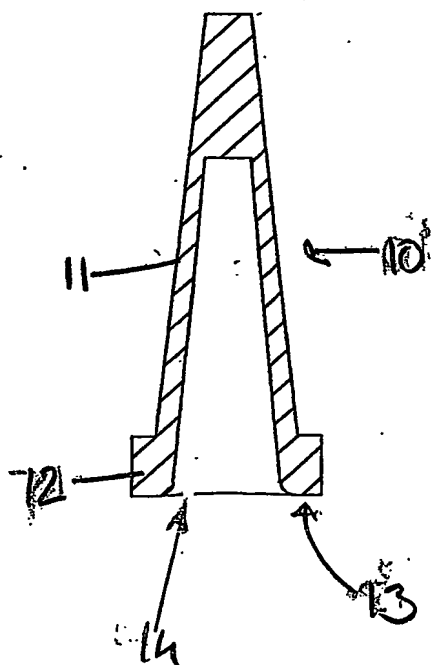


fig 6

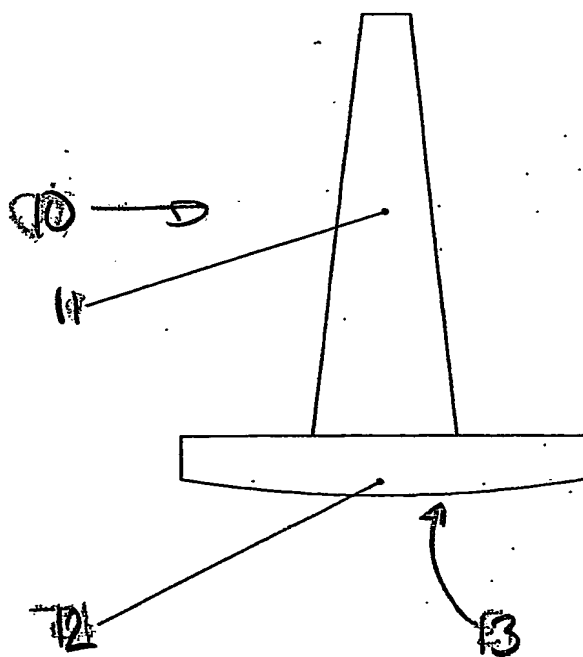


fig 5

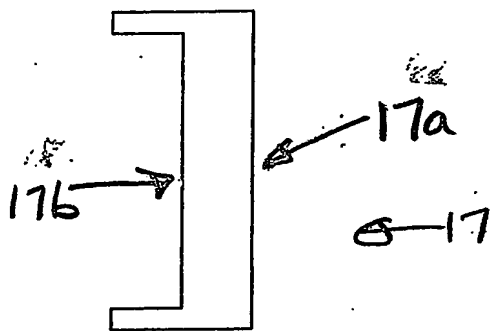


Figure 7

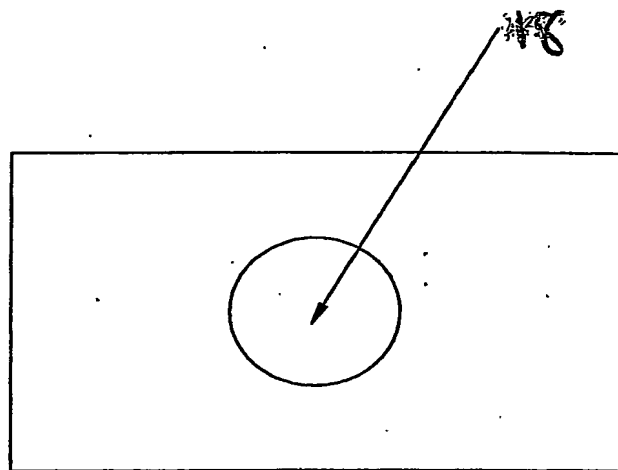


Figure 8

17

167



Figure 9

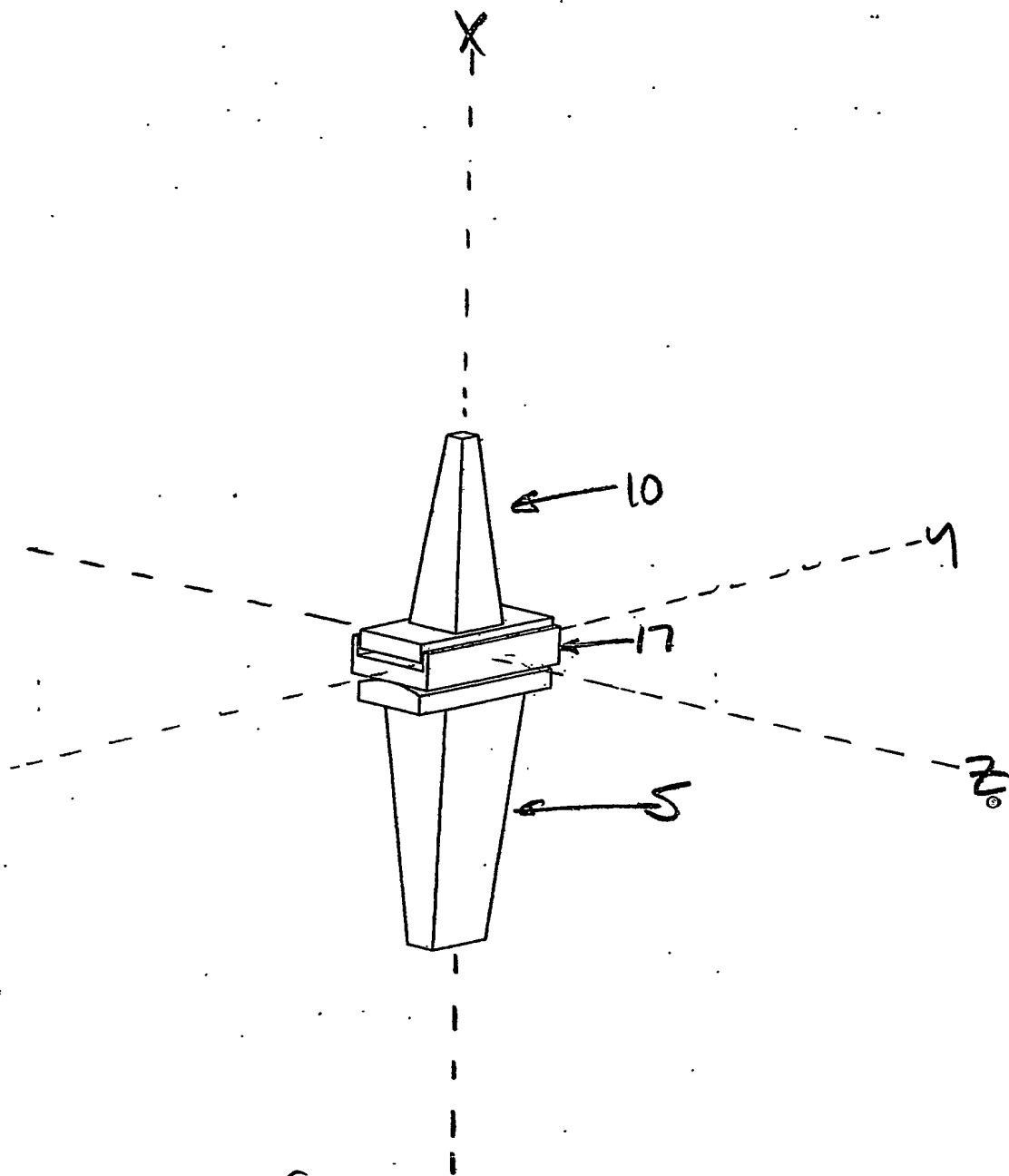


fig 10

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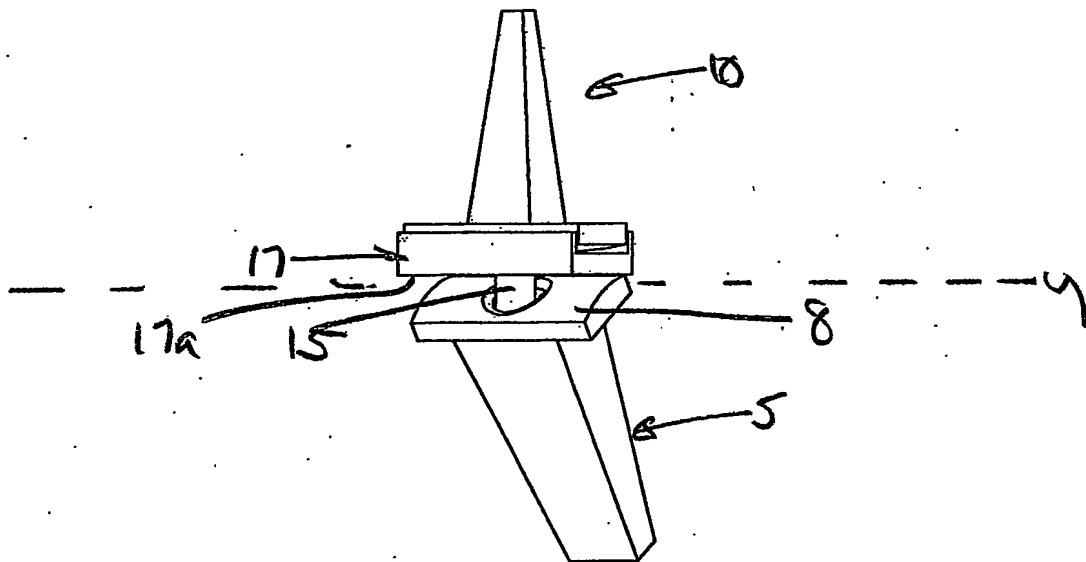


Fig. 11

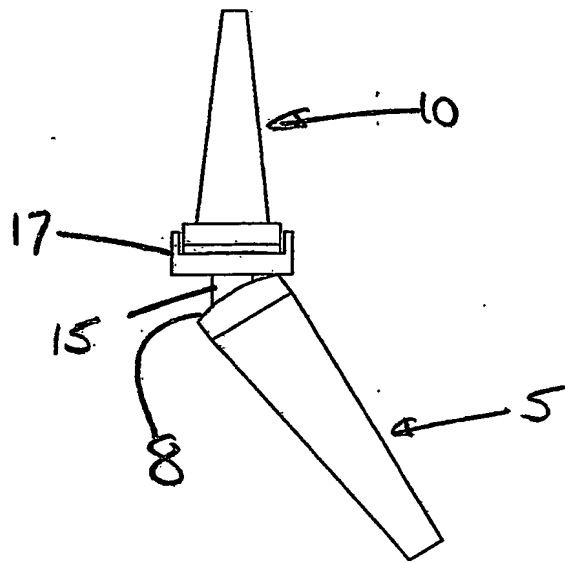


fig 12

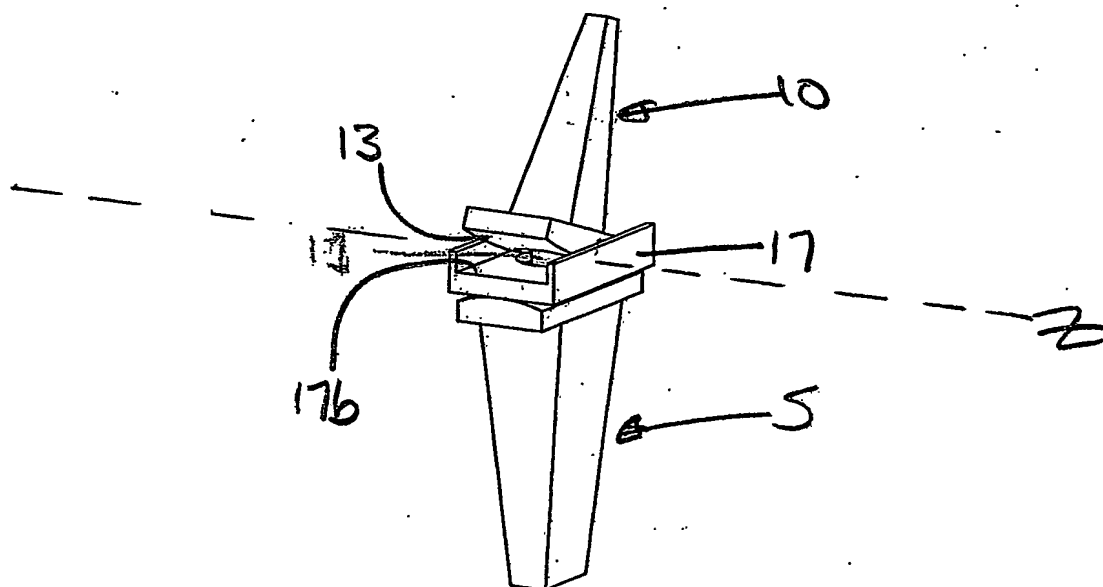


fig 13

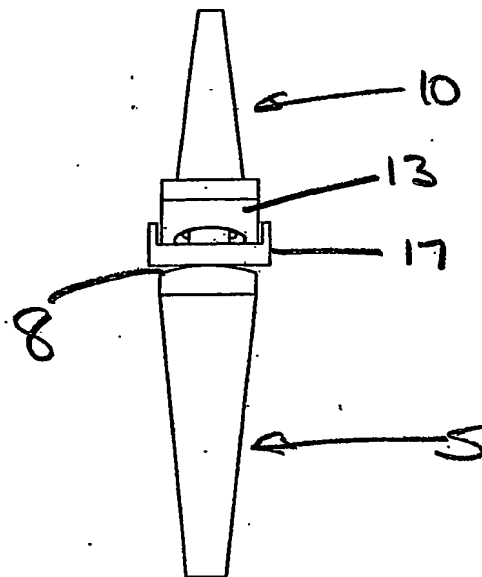


Fig. 4

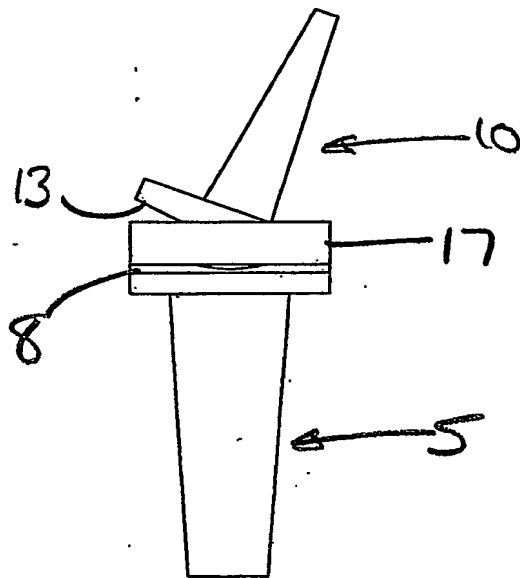


fig 15

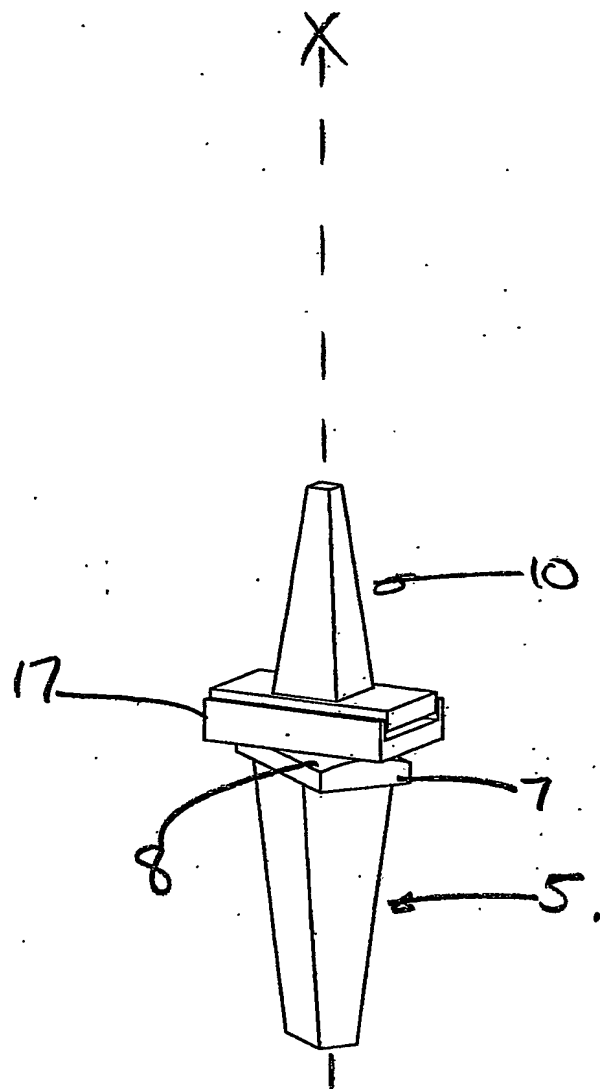


fig 6

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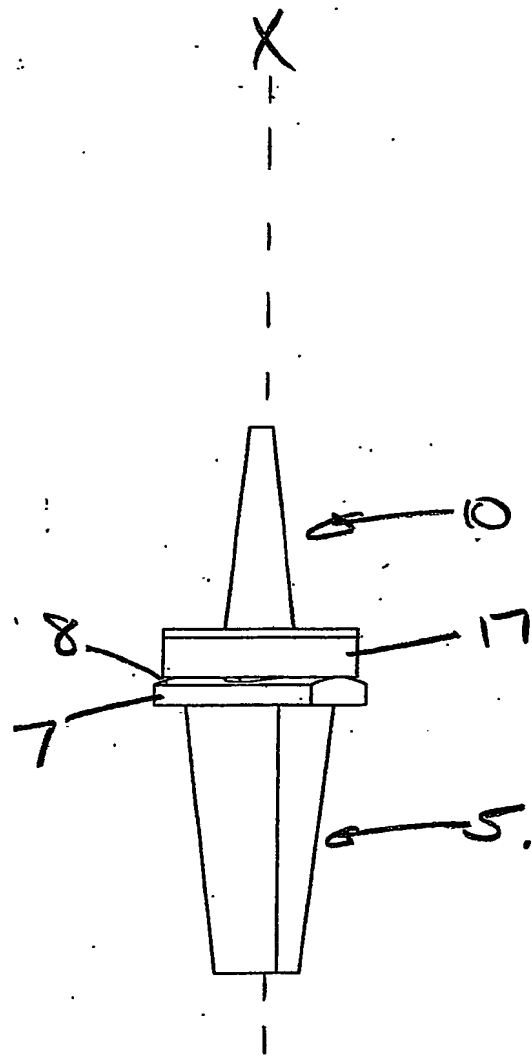


fig 17

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